

Implant Screw Breakage: A Review Article

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Abstract

Dental implants have revolutionized the treatment for edentulous and partially edentulous patients, and successful implant integration has been well documented for patients with those clinical conditions. With the high rate of implant success for edentulous individuals, the concept of osseointegration has become a predictable treatment modality^[2]. Yet this cutting-edge treatment modality is not without its own set of adversities. Implant failures are as common as implant success. The types of implant failures are 1) loss of integration, 2) positional failures 3) soft tissue defects, and 4) biomechanical failures. In this article we come to the conclusion that the mechanical stability of the implant is a multi-factorial aspect.

Keywords : *Dental Implant, Screw Breakage, Fatigue, Biomechanical Failure*

Introduction

During the past few decades dental implants have come a long way from the implants used and studied by Dr. P. Brånemark in 1978. He was the 1st person to observe and thus describe the concept of osseointegration. Although the credit of 1st ever dental implant to be used in recorded history goes to the amazing Mayan civilization in 600AD, where they successfully used pieces of shell as replacement for mandibular teeth. Many more physicians, scientists and dentists have over the centuries helped to make dental implantology as it is today, a very reliable rehabilitation method for edentulous spaces in both the maxilla and mandible. Yet this modern method although so refined, has immense potential for failures as well. As many cases fail as the number of successful cases. Clinical observations have indicated that the major causes of implant failure are (a) deficient osseointegration, (b) complication of the neighboring soft tissues (peri-mucositis and periimplantitis) and (c) mechanical complications. Among the biomechanical problems, screw loosening, abutment rotation, and abutment fracture are the major issues^[2]. We shall now go into more details about abutment fractures and the physical factors that resist as well as cause it.

Methodology

Pubmed database was searched for the keywords ‘IMPLANTS BREAKAGE’ ‘IMMEDIATE IMPLANTS’, ‘FATE OF IMPLANTS’ 141 articles were found.

Out of the 141 articles, the non dental articles were excluded to get 36 articles.

The duplicates were excluded to get 2 articles

These 4 articles were then reviewed and data for this Review Article was obtained.

DISCUSSION

Many of the materials used to restore implants are derived from conventional restorative dentistry, for example denture base resins. Complete denture wearers develop relatively little bite force compared to force generated with implant supported restorations. Breakage is a common failure of overdenture restorations (fig 1 & 2)^[1].



Fig 1: Teeth broken off an overdenture prosthesis^[1]



Fig 2: Fractured overdentures are a common failure due to increased forces and thinning of acrylic bases to accommodate implant components and tissue bars^[1]

Metal fatigue of restorative materials can also lead to breakage — the rigid connection of implants to bone demands that attention is paid to the size of connectors (Fig 3)^[1]. Breakage of implants and implant components can also occur often; this is due to poor treatment planning and exposing implants to excessive forces. The implant in Figures 4 and 5 was treatment planned as a single implant in an incomplete dentition and a terminal tooth. The implant was connected to the tooth causing decay on the tooth, and eventually the implant to fracture under the load.



Fig 3: Intra-oral view of fractured implant tissue bar.
The cantilevered attachment has fractured^[1]



Fig 4: Implant restoration together with fractured implant component^[1]

In 2015, Sun-Young Lee, Sung-Jun Kim, Hyun-Wook An, *et al* from Institute of Science & Technology, Megagen Implant, Gyeongsan, Republic of Korea Department of Periodontology, School of Dentistry, Kyungpook National University, Daegu, Republic of Korea MIR Dental Hospital, Daegu, Republic of Korea did a study on the effect on mechanical properties due to thread depth of various lengths of dental implants. They used Commercial Titanium implants of various lengths, diameters and thread depths and Solid rigid polyurethane blocks with uniformity as an alternative to human cancellous bone. The implants were tightened with a recommended torque of 30 Ncm using a digital torque meter.^[3] The Titanium implants were tightened

with the EZ Post containing the hemispherical loading members were fixed with a specimen holder that was made from brass and clamped in the jig of a universal test machine^[3]. After the static compressive strength tests, the Titanium implants were examined macroscopically. The failure mode was observed to be deformation in the abutment and being torn horizontally at the upper side of the Titanium implant. The threads in the Titanium implants with deeper threads did not show breakage. Titanium implants with the same length and inner diameter have a similar maximum compressive strength. The mechanical strength is more related to the length and diameter than the thread depth. The failure mode was observed in the fixtures and abutments but not the

threads. The thread depth did not have a major effect on the mechanical strength. Titanium implants with deeper threads did not induce the breakage of threads applying the maximum compressive strength. Dental implants may fracture at load levels below the maximum compressive strength of the implant/abutment complex. Thus, the maximum compressive strength may suggest a standard point of acute overload. Mechanical failures of dental implants appear through a repeated loading process at low loads. The fatigue test is a general method used in the laboratory to mimic actual intraoral use. The fatigue limits of the dental implants with a diameter of 4.0 mm and thread depth of 0.6 mm (636 N) and those with a diameter of 4.0 mm and thread depth of 0.35 mm (619 N) in the fatigue test on the basis of the International Organization for Standardization (ISO 14801) were both more than 600 N. The fatigue limit of the Ti implants with deeper threads is similar to that of Ti implants with shallow thread depth. The study indicated that the Ti implants with the deeper threads have similar mechanical stability^[3].

In 2009, Cleide Gisele RIBEIRO, Maria Luiza Cabral MAIA, Susanne S. SCHERRER, *et al* from Brazil conducted a study on the fatigue resistance of dental implants based on the design of abutment-implant interface. This study demonstrated the superior fatigue resistance of external hex interface. There was no significant difference between the conical and internal hex interfaces. Probably, the quality of the surface machining of the flat-to-flat mating surfaces (mainly, the machining accuracy of the screw and thread) determined the superior resistance of the connector; The mode and region of fracture in prosthetic screws observed in this study suggested that failure of these screws occurred by fatigue (presence of fatigue striations) and involved the threaded part^[2].

Conclusion

Thus, we can now see that the possibility of implant screw fracture is dependent on an array of various factors

such as technique, material, design and the peri-implant environment as well. Since titanium implants are so very much biocompatible, they can be left as it is, without any complications, if a fracture does occur and it is not feasible to remove the fractured implant.

Ethical Clearance – Not required since it is a review article

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Conflict of Interest – Nil

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